

# Grading Glaucoma Stages using Wavelet Transform

Salil Kumar Malla,  
College of Engineering Bhubaneswar

**Abstract**—A persistent eye condition called glaucoma damages the optic nerve and can result in irreversible vision loss. The traditional instrument approaches for glaucoma detection are laborious and tedious. Recently, a number of methods for automatically classifying glaucoma using retinal fundus pictures have been proposed. Nevertheless, none of the current techniques is effective for early-stage glaucoma identification. We presented a novel approach to classifying glaucoma in this letter, based on the recently developed two-dimensional tensor empirical wavelet transform (2D-T-EWT). In this study, 2D-T-EWT is used to breakdown the pre-processed images into sub-band images (SBIs). Next, from the decomposed SBIs, texture-based grey level-occurrence matrix (GLCM), chiphistogram, and moment invariant features were recovered. Robust features have already been chosen and ranked according to the student test algorithm. Ultimately, a trained multi-class support vector machine (MC-LS-SVM) classifier has been employed for the classification process. The experimental results demonstrate that our strategy for classifying glaucoma performed better than state-of-the-art approaches. Tenfold cross-validation was used in the suggested approach to attain the best classification accuracy of 93.65%.

**Index Terms**—Glaucoma, fundus images, empirical wavelet transform, feature extraction, multiclass classification.

## I. INTRODUCTION

GLAUCOMA is a chronic retinal disease caused due to increased intraocular pressure (IOP) in the optic nerve [1]. It thins the optic nerve and eventually causes irreversible vision loss [2]. The effect of glaucoma is gradual increases that cannot be detected earlier until the condition is at an advanced stage [3]. The World Health Organization (WHO) provides the international classification of diseases (ICD) codes. In ICD tenth revision-clinical modification (ICD-10-CM) codes, 365.71, 365.72, and 365.73 are given for the early-stage (mild stage), moderate-stage, and advanced-stage (severe stage), respectively [3], [4]. The vision loss effects with various stages of glaucoma are shown in Fig. 1.

Many diagnostic tools used in the medical departments are as follows. Tonometry is mostly used as a diagnostic tool to

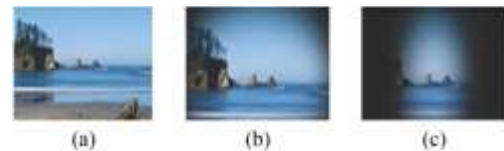


Fig. 1. Vision loss effects at various stages of glaucoma, (a) Normal (b) Early-stage glaucoma (c) Advanced-stage glaucoma.

measure IOP [5]. Perimetry is used to determine visual field loss, and stereo disc photography is helping to determine if there is unhealthy cupping in the optic nerve head (ONH) [3], [5]. These methods are laborious, sluggish, required proficient clinician. Hence, computer-based methods are needed for the early, reliable and accurate diagnosis of glaucoma.

Recently, many approaches are proposed for automatic glaucoma detection using retinal fundus. In related studies, Kirar *et al.* [6] used the concatenation of discrete wavelet transform (DWT) and empirical wavelet transform (EWT). Maheshwari *et al.* [7] and [8] Proposed EWT and variational mode decomposition (VMD) based methods, respectively. Agrawal *et al.* [9] investigated the image decomposition-based algorithm for glaucoma prediction using quasi-bivariate VMD (QB-VMD). Acharya *et al.* [10] extracted higher order spectra (HOS) and texture features from retinal images. In the different study [11], they use bi-dimensional empirical mode decomposition (BD-EMD) for extraction of entropy and energy features for glaucoma detection. Recently, Li *et al.* [12] presented a deep learning approach for glaucoma detection using a convolutional neural network (CNN) model. These methods have recently been used for the diagnosis of glaucoma. However, the classification of glaucoma stages is very crucial for the early and reliable diagnosis of glaucoma. For glaucoma classification, Noronha *et al.* [13] proposed the automatic method based on radon transform (RT) they use 272 fundus images from the private database and classified into healthy, mild, and severe glaucoma. The fundus images of various stages of glaucoma are shown in Fig. 2.

In the literature, the conventional methods [2], [11] have been used for glaucoma detection. In which DWT based algorithm [2] are non-adaptive and limited to dyadic scale. The drawbacks of the dyadic DWT based approach are as follows: Shift-invariance, constant time-frequency covering, low-frequency resolution, and signal independently. However, the conventional EMD-based method [11] having limitations such as boundary distortion, lack of mathematical theory, and mode mixing problem. Besides, EMD based decomposition highly depends

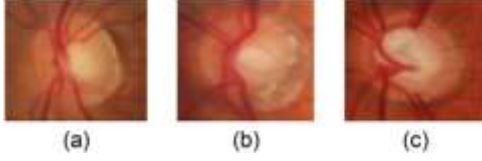


Fig. 2. Fundus images, (a) Normal image (b) Early-stage glaucoma (c) Advanced-stage glaucoma.

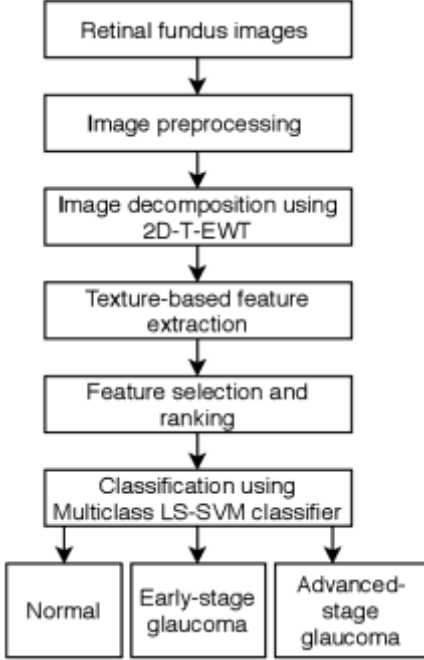


Fig. 3. The block diagram of the proposed framework.

on stopping criteria and interpolation techniques. To avoid the limitations of dyadic DWT and EMD, Gilles [18] has recently introduced a novel wavelet transform called empirical wavelet transform. Afore, Gilles *et al.* [19] extended one-dimension (1D) EWT to 2D EWT for image analysis. The EWT has various desirable properties like; it is an adaptive and signal-dependent algorithm. The main idea is to build a wavelet filter bank using Fourier supports. The advantages of the EWT as compared to the EMD is that we can adaptively use the classic wavelet for representation and EWT gives a more consistent decomposition as compared to EMD. These properties of EWT inspired us to use 2D EWT based algorithm in the proposed method for glaucoma classification. It can be observed from the literature that none of the methods can be applied over a public database. The block diagram of the proposed framework is shown in Fig. 3.

The main contributions of this letter are as follows. (1) A novel method is proposed for the classification of glaucoma stages using a newly introduced 2D-T-EWT image decomposition algorithm. (2) The main idea of the EWT based algorithm is to build a wavelet filter bank using Fourier supports. (3) The proposed method achieves higher classification accuracy than the existing approaches. (4) The performance of the proposed method is applied to the public database for a fair comparison. The remainder of the letter is as follows. The database and the proposed method is explained in detail in Section II. In Section III, we have discussed the experimental results. The

conclusion of the paper is provided in Section IV. The references are given in Section V.

## II. PROPOSED METHOD

### A. Database

In this study, we use 505 fundus images (255 normal and 250 glaucomatous images) from RIM-ONE [14] database for the binary classification. These images are stored in the 24-bit JPEG file format and resized with the resolution of  $240 \times 240$  pixels using bi-cubic interpolation to reduce the computational complexity. RIM-ONE database is publicly online available at <http://medimrg.webs.ull.es/>. Furthermore, we collect 867 fundus images (289 normal, 289 early-stage glaucoma, and 289 advanced-stage glaucoma) from Harvard Dataverse, V1 [15] database for the three-class classification. These fundus images are obtained from Kim's eye hospital. These images are taken using an automatic fundus camera (AFC-330 Nidek). These images were cropped at the optic nerve region with the size of  $240 \times 240$  pixels for the same resolution. These public databases serve as benchmarking data for automatic glaucoma detection.

### B. Image Decomposition using 2D-Tensor-Empirical Wavelet Transform

In this work, image preprocessing is used to improve image quality [6]–[9]. It is applied to remove inappropriate variations present in the image like noise, varying light intensity, and low contrast [2], [3]. Then, green channel images have improved using contrast limited adaptive histogram equalization. It increases a dynamic range and contrast of the input image [3], [8]. Furthermore, 2D-T-EWT is applied for image decomposition [19]. EWT is a signal-dependent approach. It cannot use predefined basis functions like in Fourier transform [17]–[19]. The basic idea is to build a wavelet tight frame, which is equivalent to an adaptive filter bank [18]. The main steps include in EWT are as follows; it detects the Fourier supports and built the corresponding wavelet and filter the input signal with the obtained filter bank to get the various SBIs [7], [17]. We use the classic wavelet transform to define EWT in which the detail coefficients are corresponding to empirical wavelets. The approximation coefficients are corresponding to the scaling function [19]–[21].

Previously, EWT based method is used in different biomedical applications [7], [17], [20], and [21]. The EWT based algorithm relies on the frequency spectrum of the signal. In the 2D-EWT based approach, we use a tensor product as for classic wavelets, which means we execute the rows and then the columns of the input image with the 1D-EWT algorithm [19]. First, we consider a mean spectrum for the rows (or the columns), then we execute the detection of the Fourier supports using this mean row spectrum. Then, we used the same filters for all rows (or columns) [18]. The 2D-T-EWT method performs the given steps [7], [19]. (We denotes the  $a$  input image,  $N_r$  is the number of filters for each row, and  $N_c$  is the number of filters for each column).

- 1) Perform the 1D FFT of each row  $i$  of  $a$ ;  $\hat{a}(i, \omega)$ ; and calculate the mean spectrum magnitude for rows:

$$\tilde{A}_{row} = \frac{1}{N_{row}} \sum_{i=0}^{N_{row}} \hat{a}(i, \omega) \quad (1)$$

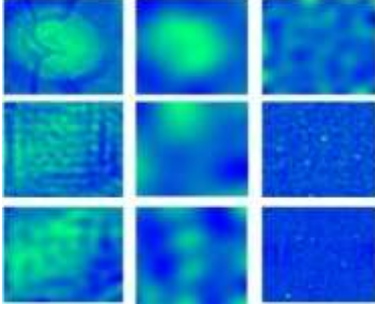


Fig.4.2D-T-EWTdecomposedcomponentsofFig.2(c),(For $N_R=3$ ,  $N_C=3$ )

- 2) Perform the 1DFFT of each column  $j$  of  $\tilde{a}$ ;  $\hat{a}(\omega, j)$ ; and calculate the mean spectrum magnitude for the column:

$$\tilde{A}_{column} = \frac{1}{N_{column}} \sum_{i=0}^{N_{column}} \hat{a}(\omega, j) \quad (2)$$

- 3) Execute the boundaries detection on  $\tilde{A}_{column}$  and build the correspondent filterbank  $\{\psi_n^{row}, \psi_n^{col}\}_{n=1}^{N_R}$
- 4) Execute the boundaries detection on  $\tilde{A}_{column}$  and build the correspondent filterbank  $\{\psi_n^{row}, \psi_n^{col}\}_{n=1}^{N_C}$
- 5) Filter  $a$  along the rows with  $\{\psi_n^{row}\}_{n=1}^{N_R}$  which provides  $N_R+1$  output images,
- 6) Filter each earlier resultant image along with the columns with  $\{\psi_n^{col}\}_{n=1}^{N_C}$ , this gives at the end  $(N_R+1)(N_C+1)$  sub-band images.

In this study, the preprocessed images are decomposed into different SBIs using 2D-T-EWT. The EWT decomposed sub-band images of Fig.2(c) are shown in Fig.4, for advanced-stage glaucoma image.

### C. Feature Extraction

In this study, texture-based features are extracted from the 2D-T-EWT decomposed components [6], [7]. Texture features are useful to measure smoothness, pixel regularities, and coarseness [2], [6]. The statistical approaches are employed for analysis of the spatial distribution of gray values from local features extraction. We use second-order gray level co-occurrence matrix (GLCM) [2], [9]. Four most significant GLCM features are energy, contrast, correlation, and homogeneity [6], [9]. The chip histogram features are statistical texture feature, in which six features are extracted, mean, variance, skewness, entropy [3], [8], energy, and kurtosis. We also used seven significant moment invariance features [2], [6].

### D. Feature Normalization, Selection, and Ranking

Feature normalization improves the overall performance of the machine-learning model [10], [11]. In this study, the extracted features are normalized using the z-score normalization algorithm [3], [6]–[9]. Further, the selection of robust features is helping to enhance the classification performance in terms of accuracy [3], [6].

In this study, we use the student's  $t$ -test algorithm for feature selection and ranking of the features based on the  $t$ -value [7]. We have considered features with higher  $t$ -value first because features with high  $t$ -value are more discrimination ability [7], [10]. In this work, twelve robust features are selected from

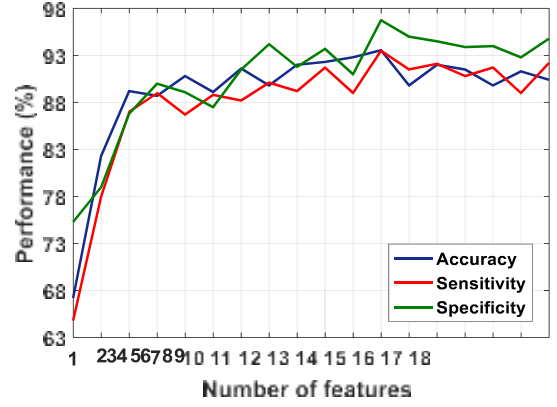


Fig.5. A graph between performance measures and the number of features for three-class classification

TABLE I  
CONFUSION MATRIX FOR BINARY CLASSIFICATION

	Normal	Glaucoma
Normal	234	21
Glaucoma	17	233

twenty-nine features, which are extracted from three different texture features set.

### E. Classification using Kernel-Based Multiclass LS-SVM Classifier

In this study, MC-LS-SVM classifier has been used for glaucoma classification. The support vector machines are a set of supervised learning algorithms, widely used as a classifier to classify two or more classes [3], [22]. In SVM, hyper-planes are employed to create a decision boundary for the classification using radial basis function (RBF) kernel [3], [6]–[10]. It can be seen from the literature that one-against-one method is more suitable than the one-against-all method for multiclass classification. To implement the one-against-one algorithm for the classifier, we consider the number of classes ( $n$  class), and then  $n \text{ class} \times (n \text{ class} - 1) / 2$  classifiers are used for each one-trained data from two stages [3], [13]. The MC-LS-SVM classifier is used in various biomedical applications such as classification of glaucoma stages [13], and classification of sleep stages based EEG signals [24].

## III. RESULTS AND DISCUSSION

In this study, 2D-T-EWT [19] image decomposition algorithm has been used for performance enhancement, because EWT [17], [18] show significant advantages over conventional methods DWT [2] and EMD [16]. In this work, the pre-processed images are decomposed into various SBIs using 2D-T-EWT [19]. Then, various texture-based features have been extracted from the decomposed components. The variation in the classification accuracy with the number of features is shown in Fig. 5. This plot shows that only twelve robust features are qualified to achieve the highest accuracy. In Fig. 6, the RBF kernel parameter ( $\sigma$ ) is varied from 0.3 to 3 with an increment of 0.3, the classification performance can be enhanced with the suitable selection of  $\sigma$  [3], [7]. The obtained confusion matrixes of the classifier after ten-fold cross-validation for binary and three-stage classification is provided in Tables I and II,

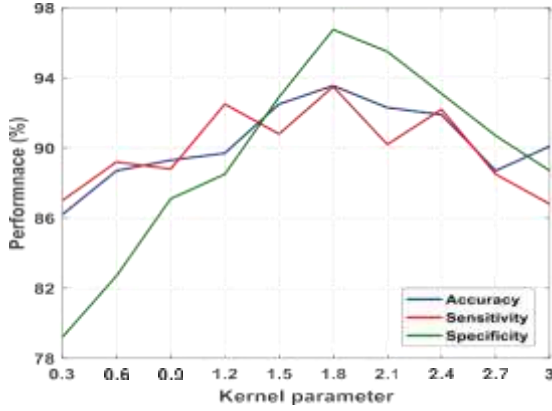


Fig. 6. A graph between performance parameters and RBF kernel parameter after tenfold cross-validation.

TABLE II  
CONFUSION MATRIX FOR THREE-CLASS CLASSIFICATION

	Normal	Early-stage	Advanced-stage
Normal	275	6	8
Early-stage	13	264	12
Advanced-stage	8	8	273

TABLE III  
CLASSIFICATION RESULTS OF THE PROPOSED METHOD ON DIFFERENT DATASETS

Database	Ac (%)	Sn (%)	Sp (%)	F2 (%)	AUC
Drishti-GS [26]	85.20	84.67	87.10	85.50	0.8589
HRF [28]	86.34	88.10	84.34	86.70	0.8622
LES-AV [29]	90.30	92.50	89.67	90.87	0.9108
RIM-ONE [14]	92.47	93.20	91.67	92.90	0.9243

respectively. In this study, five indicators are used for performance measurement namely, accuracy (Ac), sensitivity/recall (Sn), specificity (Sp) [6], [30], receiver-operating characteristic (ROC) in terms of area under the ROC (AUC), and F-score (F2) ( $F_2 = (1 + \beta^2) \times Pr \cdot Sn / (\beta^2 \cdot Pr) + Sn$ ; where Pr: precision, set  $\beta = 2$ ).

More recently, many approaches have been proposed for binary classification using RIM-ONE database. In related studies [6], [7], and [9] achieves accuracies of 83.60%, 80.66%, and 86.13%, respectively. Lately, the method [3] obtained an accuracy of 90.76%. Whereas, our method achieved the highest accuracy of 92.47% on RIM-ONE database. Besides, the effectiveness of the proposed method has been evaluated on different datasets (Drishti-GS, HRF, LES-AV, and RIM-ONE); the obtained results are shown in Table III. It can be seen from Table III, that the proposed method achieves better results on RIM-ONE database. The obtained results in terms of Ac, Sn, Sp, F2, and AUC as 92.47%, 93.20%, 91.67%, 92.90%, and 0.9243, respectively. The performance comparison of the state-of-the-art approaches on RIM-ONE database is shown in Table IV. Besides, the proposed method has been compared with advanced deep learning methods (NightOwl and WinterFell) [25]. For a fair comparison, we used three indicators Sn, Sp, and AUC. It can be seen from Table VI, that our method achieved better performance than [25], as it achieved the highest AUC of 0.9503.

For the three-class classification, Noronha *et al.* [13] reported 90.07% accuracy using SVM classifier on the private database.

TABLE IV  
PERFORMANCE COMPARISON WITH THE STATE-OF-THE-ART APPROACHES ON THE RIM-ONE DATABASE [14]

Database	Method	Ac (%)	Sn (%)	Sp (%)	F2 (%)	AUC
RIM-ONE	Maheshwari <i>et al.</i> [7]	80.66	78.00	88.23	80.90	0.8140
	Kirar <i>et al.</i> [6]	83.60	86.4	80.80	85.58	0.8357
	Agrawal <i>et al.</i> [9]	86.13	84.8	87.43	86.70	0.8710
	Parashar <i>et al.</i> [3]	90.76	94.5	87.84	90	0.9117
	<b>Ours</b>	<b>92.47</b>	<b>93.20</b>	<b>91.67</b>	<b>92.90</b>	<b>0.9243</b>

TABLE V  
PERFORMANCE OF TWO DIFFERENT METHODS FOR THREE-CLASS CLASSIFICATION ON THE SAME DATABASE [15]

Database	Method	Ac (%)	Sn (%)	Sp (%)	F2 (%)	AUC
HARVARD DATASET, V1	Noronha <i>et al.</i> [13]	88.34	87.75	91.50	88.80	0.8965
	<b>Ours</b>	<b>93.65</b>	<b>93.50</b>	<b>96.67</b>	<b>94.07</b>	<b>0.9510</b>

TABLE VI  
PERFORMANCE COMPARISON OF THE PROPOSED METHOD WITH ADVANCED DEEP LEARNING METHODS ON REFUGE TEST SET [25]

Training set	Method	Sn (%)	Sp (%)	AUC
REFUGE [25]	NightOwl [25]	90	85	0.9101
	<b>Ours</b>	<b>94.30</b>	<b>89.90</b>	<b>0.9210</b>
ORIGA [27]	WinterFell [25]	92.50	85	0.9327
	<b>Ours</b>	<b>96.40</b>	<b>93.67</b>	<b>0.9503</b>

This private database is not available as benchmarking data to evaluate image-processing algorithms for glaucoma classification. For a fair comparison, the conventional method [13] has been evaluated on the Harvard Dataverse, V1 public database. The obtained results for [13] in terms of Ac, Sn, Sp, F2, and AUC as 88.34%, 87.75%, 91.50%, 88.80%, and 0.8965 respectively. Whereas on the same database, our method achieved far better results in terms of Ac, Sn, Sp, F2, and AUC as 93.65%, 93.50%, 96.67%, 94.07%, and 0.9510, respectively. The performance comparison of the proposed method with the conventional method [13] on Harvard Dataverse, V1 database is provided in Table V. In summary, the proposed method outperformed state-of-the-art approaches for glaucoma classification.

#### IV. CONCLUSION

We employed the recently released 2D-T-EWT based algorithm for image decomposition in this letter. It was discovered that the deconstructed components of 2D-T-EWT are valuable for texture-based feature extraction. The student test algorithm is used to pick and rank these retrieved attributes. Using the MC-LS-SVM classifier, we have found that only twelve robust characteristics are qualified to attain the greatest classification accuracy. As a result, compared to the current methods, the suggested method has reduced computing complexity and more accuracy. Tenfold cross-validation has been used to assess the efficacy of the suggested approach. The findings collected demonstrate that our strategy for classifying glaucoma performed better than state-of-the-art approaches. Because the suggested method has an accuracy of 91.34% in detecting glaucoma in its early stages, it can be employed effectively and reliably for glaucoma diagnosis. In subsequent

work, we want to use deep learning models to increase classification performance.

#### REFERENCES

- [1] W. M. Liao, B. Zou, R. C. Zhao, Y. Q. Chen, Z. Y. He, and M. J. Zhou, "Clinical interpretable deep learning model for glaucoma diagnosis," *IEEE EE J. Biomed. Health Inform.*, vol. 24, no. 5, pp. 1405–1412, 2020.
- [2] B. S. Kirar, D. K. Agrawal, and S. Kirar, "Glaucoma detection using image channels and discrete wavelet transform," *IETE J. Res.*, to be published, doi:10.1080/03772063.2020.1795934.
- [3] D. Parashar and D. K. Agrawal, "Automated classification of glaucoma stages using flexible analytic wavelet transform from retinal fundus images," *IEEE Sensors J.*, vol. 20, no. 21, pp. 12885–12894, Nov. 2020.
- [4] A. T. Nguyen, D. S. Greenfield, A. S. Bhakta, J. Lee, and W. J. Feuer, "Detecting glaucoma progression using guided progression analysis with OCT and visual field assessment in eyes classified by international classification of diseases severity codes," *Amer. Acad. Ophthalmol., Ophthalmol. Glaucoma*, vol. 2, no. 1, pp. 36–46, 2019.
- [5] T. C. Lim, S. Chattopadhyay, and U. R. Acharya, "A survey and comparative study on the instruments for glaucoma detection," *Med. Eng. Phys.*, vol. 34, pp. 129–139, 2012.
- [6] B. S. Kirar and D. K. Agrawal, "Computer aided diagnosis of glaucoma using discrete and empirical wavelet transform from fundus images," *IET Image Process.*, vol. 13, no. 1, pp. 73–82, 2019.
- [7] S. Maheshwari, R. B. Pachori, and U. R. Acharya, "Automated diagnosis of glaucoma using empirical wavelet transform and correlation entropy features extracted from fundus images," *IEEE J. Biomed. Health Inform.*, vol. 21, no. 3, pp. 803–813, 2017.
- [8] S. Maheshwari, V. Kanhangad, R. B. Pachori, S. V. Bhandary, and U. R. Acharya, "Iterative variational mode decomposition based automated detection of glaucoma using fundus images," *Comput. Biol. Med.*, vol. 88, pp. 142–149, May 2017.
- [9] D. K. Agrawal, B. S. Kirar, and R. B. Pachori, "Automated glaucoma detection using quasi-bivariate mode decomposition from fundus images," *IET Image Process.*, vol. 13, no. 13, pp. 2401–2408, 2019.
- [10] U. R. Acharya, S. Dau, X. Du, and S. V. Sree, "Automated diagnosis of glaucoma using texture and higher order spectra features," *IEEE Trans. Inf. Technol. Biomed.*, vol. 15, no. 3, pp. 449–455, May 2011.
- [11] U. R. Acharya *et al.*, "Automated screening system for retinal health using bi-dimensional empirical mode decomposition and integrated index," *Comput. Biol. Med.*, vol. 75, no. 1, pp. 54–62, 2016.
- [12] L. Li *et al.*, "A large-scaled database and a CNN model for attention-based glaucoma detection," *IEEE Trans. Med. Imag.*, vol. 39, no. 2, pp. 413–424, Feb. 2020.
- [13] K. P. Noronha, U. R. Acharya, K. P. Nayak, R. J. Martis, and S. V. Bhandary, "Automated classification of glaucoma stages using higher order cumulant features," *Biomed. Signal Process. Control*, vol. 10, pp. 174–183, 2014.
- [14] F. Fumero, S. Alayon, J. L. Sanchez, J. Sigut, and M. Gonzalez-Hernandez, "RIM-ONE: An open retinal image database for optic nerve evaluation," in *Proc. 24th IEEE Int. Symp. Comput.-Based Med. Syst.*, 2011, pp. 1–6.
- [15] J. M. Ahn, S. Kim, K.-S. Ahn, S.-H. Cho, K. B. Lee, and U. S. Kim, "A deep learning model for the detection of both advanced and early glaucoma using fundus photography," *PLoS ONE*, vol. 13, no. 11, pp. 1–8, 2018, Art. no. e0207982.
- [16] N. E. Huang *et al.*, "The empirical mode decomposition and the hilbert spectrum for nonlinear and non-stationary time series analysis," *Proc. Roy. Soc. A: Math., Phys. Eng. Sci.*, vol. 454, pp. 903–995, 1998.
- [17] A. Bhattacharyya and R. B. Pachori, "A multivariate approach for patient specific EEG seizure detection using empirical wavelet transform," *IEEE Trans. Biomed. Eng.*, vol. 64, no. 9, pp. 2003–2015, Sep. 2017.
- [18] J. Gilles, "Empirical wavelet transform," *IEEE Trans. Signal Process.*, vol. 61, no. 16, pp. 3999–4010, Aug. 2013.
- [19] J. Gilles, G. Tran, and S. Osher, "2D empirical transforms: Wavelets, ridgelets, and curvelets revisited," *SIAM J. Imag. Sci.*, vol. 7, no. 1, pp. 157–186, 2014.
- [20] A. Bhattacharyya, L. Singh, and R. B. Pachori, "Fourier–Bessel series expansion based empirical wavelet transform for analysis of non-stationary signals," *Digit. Signal Process.*, vol. 78, pp. 185–196, 2018.
- [21] A. Anuragi, D. Sisodia, and R. B. Pachori, "Automated alcoholism detection using Fourier–Bessel series expansion based empirical wavelet transform," *IEEE Sensors J.*, vol. 20, no. 9, pp. 4914–4924, 2020.
- [22] J. A. K. Suykens and J. Vandewalle, "Least squares support vector machine classifiers," *Neural Process. Lett.*, vol. 9, no. 3, pp. 293–300, 1999.
- [23] S. Taran and V. Bajaj, "Sleep apnea detection using artificial bee colony optimized Hermite basis functions for EEG signals," *IEEE Trans. Instrum. Meas.*, vol. 69, no. 2, pp. 608–616, Feb. 2020.
- [24] V. Bajaj and R. B. Pachori, "Automatic classification of sleep stages based on theme-frequency image of EEG signals," *Comput. Methods Programs Biomed.*, vol. 112, no. 3, pp. 320–328, 2013.
- [25] J. I. Orlando *et al.*, "REFUGE challenge: A unified framework for evaluating automated methods for glaucoma assessment from fundus photographs," *Med. Image Anal.*, vol. 59, Jan. 2020, Art. no. 101570, doi:10.1016/j.media.2019.101570.
- [26] J. Sivaswamy, S. R. Krishnadas, G. D. Joshi, M. Jain, and A. U. S. Tabish, "Drish ti-GS: Retinal image dataset for optic nerve head (ONH) segmentation," in *Proc. IEEE 11th Int. Symp. Biomed. Imag.*, Apr./May 2014, pp. 53–56.
- [27] Z. Zhang *et al.*, "ORIGA-light: An online retinal fundus image database for glaucoma analysis and research," in *Proc. Annu. Int. Conf. IEEE Eng. Med. Biol.*, Aug./Sep. 2010, pp. 3065–3068.
- [28] J. Odstrcilik *et al.*, "Retinal vessel segmentation by improved matched filtering: Evaluation on a new high-resolution fundus image database," *IET Image Process.*, vol. 7, no. 4, pp. 373–383, Jun. 2013.
- [29] J. I. Orlando *et al.*, "Towards a glaucoma risk index based on simulated hemodynamics from fundus images," in *Proc. Int. Conf. Med. Image Comput. Assist. Interv.*, Granada, Spain, vol. 11071, 2018, pp. 65–73.
- [30] J. I. Orlando, E. Prokofyeva, and M. B. Blaschko, "A discriminatively trained fully connected conditional random field model for blood vessel segmentation in fundus images," *IEEE Trans. Biomed. Eng.*, vol. 64, no. 1, pp. 16–27, Jan. 2017.

